

# Package: eegkit (via r-universe)

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**Type** Package

**Title** Toolkit for Electroencephalography Data

**Version** 1.0-4

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**Author** Nathaniel E. Helwig <helwig@umn.edu>

**Maintainer** Nathaniel E. Helwig <helwig@umn.edu>

**Depends** R (>= 2.10), eegkitdata, bigsplines, ica, rgl, signal

**Description** Analysis and visualization tools for electroencephalography (EEG) data. Includes functions for (i) plotting EEG data, (ii) filtering EEG data, (iii) smoothing EEG data; (iv) frequency domain (Fourier) analysis of EEG data, (v) Independent Component Analysis of EEG data, and (vi) simulating event-related potential EEG data.

**License** GPL (>= 2)

**NeedsCompilation** no

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eegkit-package	<i>Toolkit for Electroencephalography Data</i>
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## Description

Analysis and visualization tools for electroencephalography (EEG) data. Includes functions for (i) plotting EEG data, (ii) filtering EEG data, (iii) smoothing EEG data; (iv) frequency domain (Fourier) analysis of EEG data, (v) Independent Component Analysis of EEG data, and (vi) simulating event-related potential EEG data.

## Details

The DESCRIPTION file:

```

Package:    eegkit
Type:      Package
Title:     Toolkit for Electroencephalography Data
Version:   1.0-4
Date:     2018-11-06
Author:    Nathaniel E. Helwig <helwig@umn.edu>
Maintainer: Nathaniel E. Helwig <helwig@umn.edu>
Depends:  eegkitdata, bigsplines, ica, rgl, signal
Description: Analysis and visualization tools for electroencephalography (EEG) data. Includes functions for (i) plotting EEG
License:   GPL (>=2)

```

Index of help topics:

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eegcapdense	Draws Dense EEG Cap with Selected Electrodes
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eegfft	Fast Fourier Transform of EEG Data
eegfilter	Filters EEG Data
eeghead	Dummy Head for 3d EEG Plots
eegica	Independent Component Analysis of EEG Data
eegkit-package	Toolkit for Electroencephalography Data
eegmesh	EEG Cap for Dense Coordinates

eegpsd	Plots Power Spectral Density of EEG Data
eegresample	Change Sampling Rate of EEG Data
eegsim	Simulate Event-Related Potential EEG Data
eegsmooth	Spatial and/or Temporal Smoothing of EEG Data
eegspace	Plots Multi-Channel EEG Spatial Map
eegtime	Plots Single-Channel EEG Time Course
eegtimec	Plots Multi-Channel EEG Time Course

### Author(s)

Nathaniel E. Helwig <helwig@umn.edu>

Maintainer: Nathaniel E. Helwig <helwig@umn.edu>

### References

- Adler, D., Murdoch, D., and others (2014). *rgl: 3D visualization device system (OpenGL)*. <http://CRAN.R-project.org/package=rgl>
- Bache, K. & Lichman, M. (2013). UCI Machine Learning Repository [<http://archive.ics.uci.edu/ml>]. Irvine, CA: University of California, School of Information and Computer Science.
- Begleiter, H. *Neurodynamics Laboratory*. State University of New York Health Center at Brooklyn. <http://www.downstate.edu/hbntl/>
- Bell, A.J. & Sejnowski, T.J. (1995). An information-maximization approach to blind separation and blind deconvolution. *Neural Computation*, 7, 1129-1159.
- Cardoso, J.F., & Souloumiac, A. (1993). Blind beamforming for non-Gaussian signals. *IEE Proceedings-F*, 140, 362-370.
- Cardoso, J.F., & Souloumiac, A. (1996). Jacobi angles for simultaneous diagonalization. *SIAM Journal on Matrix Analysis and Applications*, 17, 161-164.
- Cooley, James W., and Tukey, John W. (1965) An algorithm for the machine calculation of complex Fourier series, *Math. Comput.* 19(90), 297-301.
- Harrell, F., Dupont, C., and Others. *Hmisc: Harrell Miscellaneous*. <http://CRAN.R-project.org/package=Hmisc>
- Helwig, N. E. (2013). *Fast and stable smoothing spline analysis of variance models for large samples with applications to electroencephalography data analysis*. Unpublished doctoral dissertation. University of Illinois at Urbana-Champaign.
- Helwig, N.E. (2018). *bigsplines: Smoothing Splines for Large Samples*. <http://CRAN.R-project.org/package=bigsplines>
- Helwig, N.E. (2018). *ica: Independent Component Analysis*. <http://CRAN.R-project.org/package=ica>
- Helwig, N. E., Hong, S., Hsiao-Wecksler E. T., & Polk, J. D. (2011). Methods to temporally align gait cycle data. *Journal of Biomechanics*, 44(3), 561-566.
- Helwig, N.E. & Hong, S. (2013). A critique of Tensor Probabilistic Independent Component Analysis: Implications and recommendations for multi-subject fMRI data analysis. *Journal of Neuroscience Methods*, 213, 263-273.
- Helwig, N. E. & Ma, P. (2015). Fast and stable multiple smoothing parameter selection in smoothing spline analysis of variance models with large samples. *Journal of Computational and Graphical Statistics*, 24(3), 715-732.

Helwig, N. E. & Ma, P. (2016). Smoothing spline ANOVA for super large samples: Scalable computation via rounding parameters. *Statistics and Its Interface*, 9(4), 433-444.

Ingber, L. (1997). Statistical mechanics of neocortical interactions: Canonical momenta indicators of electroencephalography. *Physical Review E*, 55, 4578-4593.

Ingber, L. (1998). Statistical mechanics of neocortical interactions: Training and testing canonical momenta indicators of EEG. *Mathematical Computer Modelling*, 27, 33-64.

Oostenveld, R., and Praamstra, P. (2001). The Five percent electrode system for high-resolution EEG and ERP measurements. *Clinical Neurophysiology*, 112, 713-719.

Schlager, S. & authors of VCGLIB. (2014). Rvcg: Manipulations of triangular meshes (smoothing, quadric edge collapse decimation, im- and export of various mesh file-formats, cleaning, etc.) based on the VCGLIB API. R package version 0.7.1. <http://CRAN.R-project.org/package=Rvcg>.

Singleton, R. C. (1979) Mixed Radix Fast Fourier Transforms, in Programs for Digital Signal Processing, IEEE Digital Signal Processing Committee eds. IEEE Press.

## See Also

[eegkitdata](#)

## Examples

```
# See eegcap, eegcapdense, eegfft, eegica, eegresample,
# eegsim, eegsmooth, eegspace, eegtime, and eegtimemc
```

---

eegcap

*Draws EEG Cap with Selected Electrodes*

---

## Description

Creates two- or three-dimensional plot of electroencephalography (EEG) cap with user-input electrodes. Three-dimensional plots are created using the [eegcoord](#) data and the [plot3d](#) function (from [rgl](#) package). Currently supports 84 scalp electrodes, and plots according to the international 10-10 system. Includes customization options (e.g., each electrode can have a unique plotting color, size, label color, etc.).

## Usage

```
eegcap(electrodes = "10-10", type = c("2d", "3d"),
       plotlabels = TRUE, plotaxes = FALSE, main = "",
       xyzlab = NULL, cex.point = NULL, col.point = NULL,
       col.border = NULL, cex.label = NULL, col.label = NULL,
       nose = TRUE, ears = TRUE, head = TRUE,
       col.head = "AntiqueWhite", index = FALSE,
       plt = c(0.03,0.97,0.03,0.97), ...)
```

**Arguments**

electrodes	Character vector with electrodes to plot. Each element of electrodes must match one of the 89 reference electrodes (see Notes). Mismatches are ignored (not plotted). Input is NOT case sensitive. Default plots all available electrodes (full 10-10 system).
type	Type of plot to create: type="3d" produces three-dimensional plot, whereas type="2d" produces two-dimensional projection plot (bird's eye view).
plotlabels	If TRUE, the electrode labels are plotted.
plotaxes	If TRUE, the axes are plotted.
main	Title to use for plot. Default is no title
xyzlab	Axis labels to use for plot. If type="2d", then xyzlab should be two-element character vector giving x and y axis labels. If type="3d", then xyzlab should be three-element character vector giving x, y, and z axis labels.
cex.point	Size of electrode points. Can have a unique size for each electrode.
col.point	Color of electrode points. Can have a unique color for each electrode.
col.border	Color of electrode point borders. Can have a unique color for each electrode.
cex.label	Size of electrode labels. Can have a unique size for each electrode label. Input is ignored if plotlabels=FALSE is used.
col.label	Color of electrode labels. Can have a unique color for each electrode label. Input is ignored if plotlabels=FALSE is used.
nose	If TRUE, triangle is plotted to represent the subject's nose. Ignored if type="3d".
ears	If TRUE, ovals are plotted to represent the subject's ears. Ignored if type="3d".
head	If TRUE, head is plotted. Ignored if type="2d".
col.head	Color for dummy head in 3d plot. Ignored if type="2d".
index	Logical indicating if the cap row indices should be returned (see Note).
plt	A vector of the form c(x1, x2, y1, y2) giving the coordinates of the plot region as fractions of the current figure region. See <a href="#">par</a> .
...	Optional inputs for plot or plot3d function.

**Value**

Produces plot of EEG cap and possibly returns cap row indices.

**Note**

Currently supports 84 scalp electrodes (plus ears and nose): A1 A2 AF1 AF2 AF3 AF4 AF5 AF6 AF7 AF8 AFZ C1 C2 C3 C4 C5 C6 CP1 CP2 CP3 CP4 CP5 CP6 CPZ CZ F1 F2 F3 F4 F5 F6 F7 F8 F9 F10 FC1 FC2 FC3 FC4 FC5 FC6 FCZ FP1 FP2 FPZ FT7 FT8 FT9 FT10 FZ I1 I2 IZ NZ O1 O2 OZ P1 P2 P3 P4 P5 P6 P7 P8 P9 P10 PO1 PO2 PO3 PO4 PO5 PO6 PO7 PO8 PO9 PO10 POZ PZ T7 T8 T9 T10 TP7 TP8 TP9 TP10

See [eegcoord](#) for the coordinates used to create plot. Setting index=TRUE returns the row indices of [eegcoord](#) that were used to plot the cap.

To save three-dimensional plots, use the [rgl.postscript](#) function (from rgl package).

**Author(s)**

Nathaniel E. Helwig <helwig@umn.edu>

**References**

Adler, D., Murdoch, D., and others (2014). *rgl: 3D visualization device system (OpenGL)*. <http://CRAN.R-project.org/package=rgl>

Oostenveld, R., and Praamstra, P. (2001). The Five percent electrode system for high-resolution EEG and ERP measurements. *Clinical Neurophysiology*, 112, 713-719.

**Examples**

```
##### EXAMPLE 1 #####

# plot 10-10 system (default):

# plot full cap 2d (default options)
eegcap()

# plot full cap 2d (different color for ears and nose)
data(eegcoord)
mycols <- rep("white",87)
enames <- rownames(eegcoord)
mycols[enames=="A1"] <- "green"
mycols[enames=="A2"] <- "light blue"
mycols[enames=="NZ"] <- "pink"
eegcap(col.point = mycols)

##### EXAMPLE 2 #####

# plot 10-20 system:

# plot 2d cap with labels
eegcap("10-20")

# plot 2d cap without labels
eegcap("10-20", plotlabels = FALSE)

##### EXAMPLE 3 #####

# plot custom subset of electrodes
myelectrodes <- c("FP1", "FP2", "FPZ", "F7", "F3", "FZ",
                 "F4", "F8", "T7", "C3", "CZ", "C4", "T8",
                 "P7", "P3", "PZ", "P4", "P8", "O1", "O2")
eegcap(myelectrodes)
```

eegcap2d

*Draws 2D EEG Cap***Description**

Creates two-dimensional plot of electroencephalography (EEG) cap with user-input electrodes. Currently supports 84 scalp electrodes, and plots according to the international 10-10 system. Includes customization options (e.g., each electrode can have a unique plotting color, size, label color, etc.).

**Usage**

```
eegcap2d(electrodes = "10-10", axes = FALSE, asp = 1,
         cex.point = 2.75, col.point = "green", pch.point = 19,
         cex.border = 2.75, col.border = "black", pch.border = 21,
         cex.label = 0.5, col.label = "black",
         head = TRUE, nose = TRUE, ears = TRUE,
         main = "", xlab = "", ylab = "",
         xlim = c(-13.7, 13.7), ylim = c(-13.7, 13.7), ...)
```

**Arguments**

electrodes	Character vector with electrodes to plot. Each element of electrodes must match one of the 89 reference electrodes (see Details). Mismatches are ignored (not plotted). Input is NOT case sensitive. Default plots all available electrodes (full 10-10 system).
axes	If FALSE (default), no axes are plotted.
asp	Aspect ratio for plot (defaults to 1).
cex.point	Character EXpansion value for electrodes. Set to a negative value to suppress the electrode plotting.
col.point	Color for electrodes. Ignored if cex.point < 0.
pch.point	Plotting character for electrodes. Ignored if cex.point < 0.
cex.border	Character EXpansion value for electrode borders. Set to a negative value to suppress the electrode border plotting.
col.border	Color for electrode borders. Ignored if cex.border < 0.
pch.border	Plotting character for electrode borders. Ignored if cex.border < 0.
cex.label	Character EXpansion value for electrode labels. Set to a negative value to suppress the electrode label plotting.
col.label	Color for electrode labels. Ignored if cex.label < 0.
head	If TRUE, a circle is plotted to represent the subject's head.
nose	If TRUE, a triangle is plotted to represent the subject's nose.
ears	If TRUE, two ovals are plotted to represent the subject's ears.
main	Title to use for plot. Default is no title.

xlab, ylab	x-axis and y-axis labels for the plot. Default is no axis labels.
xlim, ylim	x-axis and y-axis limits for the plot.
...	Optional inputs for plot function.

### Details

Currently supports 84 scalp electrodes (plus ears and nose): A1 A2 AF1 AF2 AF3 AF4 AF5 AF6 AF7 AF8 AFZ C1 C2 C3 C4 C5 C6 CP1 CP2 CP3 CP4 CP5 CP6 CPZ CZ F1 F2 F3 F4 F5 F6 F7 F8 F9 F10 FC1 FC2 FC3 FC4 FC5 FC6 FCZ FP1 FP2 FPZ FT7 FT8 FT9 FT10 FZ I1 I2 IZ NZ O1 O2 OZ P1 P2 P3 P4 P5 P6 P7 P8 P9 P10 PO1 PO2 PO3 PO4 PO5 PO6 PO7 PO8 PO9 PO10 POZ PZ T7 T8 T9 T10 TP7 TP8 TP9 TP10

See [eegcoord](#) for the coordinates used to create plot.

### Value

Produces plot of EEG cap.

### Note

Unlike the [eegcap](#) function, this function does not use `par$plt` for the figure positioning.

### Author(s)

Nathaniel E. Helwig <helwig@umn.edu>

### References

Oostenveld, R., and Praamstra, P. (2001). The Five percent electrode system for high-resolution EEG and ERP measurements. *Clinical Neurophysiology*, 112, 713-719.

### See Also

See [eegcap](#) for a similar implementation, which also supports 3d EEG cap plotting.

### Examples

```
##### EXAMPLE 1 #####

# plot 10-10 system (default):

# plot full cap (default options)
eegcap2d()

# plot full cap (different color for ears and nose)
data(eegcoord)
mycols <- rep(NA, 87)
enames <- rownames(eegcoord)
mycols[enames=="A1"] <- "green"
mycols[enames=="A2"] <- "light blue"
mycols[enames=="NZ"] <- "pink"
```



```
eegcap2d(col.point = mycols)

##### EXAMPLE 2 #####

# plot 10-20 system:

# plot cap with labels
eegcap2d("10-20")

# plot cap without labels
eegcap2d("10-20", cex.label = -1)

##### EXAMPLE 3 #####

# plot custom subset of electrodes
myelectrodes <- c("FP1", "FP2", "FPZ", "F7", "F3", "FZ",
                 "F4", "F8", "T7", "C3", "CZ", "C4", "T8",
                 "P7", "P3", "PZ", "P4", "P8", "O1", "O2")
eegcap2d(myelectrodes)
```

---

eegcapdense

*Draws Dense EEG Cap with Selected Electrodes*


---

## Description

Creates two- or three-dimensional plot of dense electroencephalography (EEG) cap that spans user-input electrodes. Three-dimensional plots are created using the [eegdense](#) data and the [plot3d](#) function (from [rgl](#) package). Currently supports 933 scalp electrodes. Includes customization options (e.g., each electrode can have a unique plotting color, size, label color, etc.).

## Usage

```
eegcapdense(electrodes = "10-10", type = c("2d", "3d"),
            plotlabels = TRUE, plotaxes = FALSE, main = "",
            xyzlab = NULL, cex.point = NULL, col.point = NULL,
            cex.label = NULL, col.label = NULL, nose = TRUE,
            ears = TRUE, head = TRUE, col.head = "AntiqueWhite",
            index = FALSE, zconst = 0.5, plt = c(0.03, 0.97, 0.03, 0.97), ...)
```

## Arguments

**electrodes** Character vector with electrodes to plot. Each element of `electrodes` must match one of the 89 reference electrodes (see Notes). Mismatches are ignored (not plotted). Input is NOT case sensitive. Default plots all available electrodes (full 10-10 system).

type	Type of plot to create: type="3d" produces three-dimensional plot, whereas type="2d" produces two-dimensional projection plot (bird's eye view).
plotlabels	If TRUE, the electrode labels are plotted.
plotaxes	If TRUE, the axes are plotted.
main	Title to use for plot. Default is no title
xyzlab	Axis labels to use for plot. If type="2d", then xyzlab should be two-element character vector giving x and y axis labels. If type="3d", then xyzlab should be three-element character vector giving x, y, and z axis labels.
cex.point	Size of electrode points. Can have a unique size for each electrode.
col.point	Color of electrode points. Can have a unique color for each electrode.
cex.label	Size of electrode labels. Can have a unique size for each electrode label. Input is ignored if plotlabels=FALSE is used.
col.label	Color of electrode labels. Can have a unique color for each electrode label. Input is ignored if plotlabels=FALSE is used.
nose	If TRUE, triangle is plotted to represent the subject's nose. Ignored if type="3d".
ears	If TRUE, ovals are plotted to represent the subject's ears. Ignored if type="3d".
head	If TRUE, head is plotted. Ignored if type="2d".
col.head	Color for dummy head in 3d plot. Ignored if type="2d".
index	Logical indicating if the cap row indices should be returned (see Note).
zconst	Scalar controlling which row indices should be returned (see Note).
plt	A vector of the form c(x1, x2, y1, y2) giving the coordinates of the plot region as fractions of the current figure region. See <a href="#">par</a> .
...	Optional inputs for plot or plot3d function.

**Value**

Produces plot of EEG cap and possibly returns cap row indices.

**Note**

Currently supports 84 scalp electrodes (plus ears and nose): A1 A2 AF1 AF2 AF3 AF4 AF5 AF6 AF7 AF8 AFZ C1 C2 C3 C4 C5 C6 CP1 CP2 CP3 CP4 CP5 CP6 CPZ CZ F1 F2 F3 F4 F5 F6 F7 F8 F9 F10 FC1 FC2 FC3 FC4 FC5 FC6 FCZ FP1 FP2 FPZ FT7 FT8 FT9 FT10 FZ I1 I2 IZ NZ O1 O2 OZ P1 P2 P3 P4 P5 P6 P7 P8 P9 P10 PO1 PO2 PO3 PO4 PO5 PO6 PO7 PO8 PO9 PO10 POZ PZ T7 T8 T9 T10 TP7 TP8 TP9 TP10

See [eegdense](#) for the coordinates used to create plot. Setting index=TRUE returns the row indices of [eegdense](#) that were used to plot the cap. Only returns row indices with z-coordinates >= (zmin-zconst), where zmin is minimum z-coordinate of input electrodes.

To save three-dimensional plots, use the [rgl.postscript](#) function (from rgl package).

**Author(s)**

Nathaniel E. Helwig <helwig@umn.edu>

## References

Adler, D., Murdoch, D., and others (2014). *rgl: 3D visualization device system (OpenGL)*. <http://CRAN.R-project.org/package=rgl>

Oostenveld, R., and Praamstra, P. (2001). The Five percent electrode system for high-resolution EEG and ERP measurements. *Clinical Neurophysiology*, 112, 713-719.

## Examples

```
##### EXAMPLE 1 #####
```

```
# plot 10-10 system (default):
eegcapdense()
```

```
##### EXAMPLE 2 #####
```

```
# plot 10-20 system:
eegcapdense("10-20", plotlabels = FALSE)
```

```
##### EXAMPLE 3 #####
```

```
# plot custom subset of electrodes
myelectrodes <- c("FP1", "FP2", "FPZ", "F7", "F3", "FZ",
                 "F4", "F8", "T7", "C3", "CZ", "C4", "T8",
                 "P7", "P3", "PZ", "P4", "P8", "O1", "O2")
eegcapdense(myelectrodes)
```

---

eegcoord

*EEG Cap Coordinates*

---

## Description

Three-dimensional electroencephalography (EEG) electrode coordinates (measured in cm), and corresponding projection onto two-dimensional xy plane. Contains 84 scalp electrodes, as well as nose and ears.

## Usage

```
data(eegcoord)
```

## Format

A data frame with 87 observations and the following 5 variables:

**x** x-coordinate of 3d cap (numeric).

**y** y-coordinate of 3d cap (numeric).

**z** z-coordinate of 3d cap (numeric).

**xproj** Projected x-coordinate of 2d cap (numeric).

**yproj** Projected y-coordinate of 2d cap (numeric).

Electrode channel name labels can be obtained using `rownames(eegcoord)`.

### Author(s)

Nathaniel E. Helwig <helwig@umn.edu>

### Source

Created by Nathaniel E. Helwig (2014) using:

Adler, D., Murdoch, D., and others (2014). *rgl: 3D visualization device system (OpenGL)*. <http://CRAN.R-project.org/package=rgl>

Oostenveld, R., and Praamstra, P. (2001). The Five percent electrode system for high-resolution EEG and ERP measurements. *Clinical Neurophysiology*, 112, 713-719.

Schlager, S. & authors of VCGLIB. (2014). Rvcg: Manipulations of triangular meshes (smoothing, quadric edge collapse decimation, im- and export of various mesh file-formats, cleaning, etc.) based on the VCGLIB API. R package version 0.7.1. <http://CRAN.R-project.org/package=Rvcg>.

### Examples

```
##### EXAMPLE #####

data(eegcoord)
enames <- rownames(eegcoord)
# plot3d(eegcoord[,1],eegcoord[,2],eegcoord[,3],size=10,col="green")
# text3d(eegcoord[,1],eegcoord[,2],eegcoord[,3],texts=enames,col="blue")
plot(eegcoord[,4],eegcoord[,5],cex=2,col="green",pch=19)
text(eegcoord[,4],eegcoord[,5],labels=enames,col="blue")
```

---

eegdense

*Dense EEG Cap Coordinates*

---

### Description

Dense (hypothetical) three-dimensional electroencephalography (EEG) electrode coordinates, and corresponding projection onto two-dimensional plane. Dense cap spans the 84 scalp electrodes defined in [eegcoord](#).

### Usage

```
data(eegdense)
```

**Format**

A data frame with 977 observations and the following 5 variables:

**x** x-coordinate of 3d cap (numeric).

**y** y-coordinate of 3d cap (numeric).

**z** z-coordinate of 3d cap (numeric).

**xproj** Projected x-coordinate of 2d cap (numeric).

**yproj** Projected y-coordinate of 2d cap (numeric).

**Author(s)**

Nathaniel E. Helwig <helwig@umn.edu>

**Source**

Created by Nathaniel E. Helwig (2014) using:

Adler, D., Murdoch, D., and others (2014). *rgl: 3D visualization device system (OpenGL)*. <http://CRAN.R-project.org/package=rgl>

Oostenveld, R., and Praamstra, P. (2001). The Five percent electrode system for high-resolution EEG and ERP measurements. *Clinical Neurophysiology*, 112, 713-719.

Schlager, S. & authors of VCGLIB. (2014). Rvcg: Manipulations of triangular meshes (smoothing, quadric edge collapse decimation, im- and export of various mesh file-formats, cleaning, etc.) based on the VCGLIB API. R package version 0.7.1. <http://CRAN.R-project.org/package=Rvcg>.

**Examples**

```
##### EXAMPLE #####
data(eegdense)
# plot3d(eegdense[,1],eegdense[,2],eegdense[,3],size=10,col="green")
plot(eegdense[,4],eegdense[,5],cex=1,col="green",pch=19)
```

---

eegfft

*Fast Fourier Transform of EEG Data*

---

**Description**

Finds the strength (amplitude) and phase shift of the input signal(s) at a particular range of frequencies via a Discrete Fast Fourier Transform (FFT). Can input single or multi-channel data.

**Usage**

```
eegfft(x, Fs, lower, upper)
```

**Arguments**

<code>x</code>	Vector or matrix (time by channel) of EEG data with $n$ time points.
<code>Fs</code>	Sampling rate of <code>x</code> in Hz such that $n = s * Fs$ where $s$ is the number of seconds of input data (some positive integer).
<code>lower</code>	Lower band in Hz. Smallest frequency to keep (defaults to 0).
<code>upper</code>	Upper band in Hz. Largest frequency to keep (defaults to $Fs/2 - Fs/n$ ).

**Details**

The `fft` function (or `mvfft` function) is used to implement the FFT (or multivariate FFT). Given the FFT, the *strength* of the signal is the modulus (`Mod`), and the *phase.shift* is the angle (`Arg`).

**Value**

If `x` is a vector, returns a data frame with variables:

<code>frequency</code>	vector of frequencies
<code>strength</code>	strength (amplitude) of signal at each frequency
<code>phase.shift</code>	phase shift of signal at each frequency

If `x` is a matrix with  $J$  channels, returns a list with elements:

<code>frequency</code>	vector of frequencies of length $F$
<code>strength</code>	$F$ by $J$ matrix: strength (amplitude) of signal at each frequency and channel
<code>phase.shift</code>	$F$ by $J$ matrix: phase shift of signal at each frequency and channel

**Note**

The strength of the signal has the same unit as the input (typically microvolts), and the phase shift is measured in radians (range  $-pi$  to  $pi$ ).

**Author(s)**

Nathaniel E. Helwig <helwig@umn.edu>

**References**

- Cooley, James W., and Tukey, John W. (1965) An algorithm for the machine calculation of complex Fourier series, *Math. Comput.* 19(90), 297-301.
- Singleton, R. C. (1979) Mixed Radix Fast Fourier Transforms, in *Programs for Digital Signal Processing*, IEEE Digital Signal Processing Committee eds. IEEE Press.

**Examples**

```
##### EXAMPLE #####

### Data Generation ###

# parameters for signal
Fs <- 1000 # 1000 Hz signal
s <- 3 # 3 seconds of data
t <- seq(0, s - 1/Fs, by = 1/Fs) # time sequence
n <- length(t) # number of data points
freqs <- c(1, 5, 10, 20) # frequencies
amp <- c(2, 1.5, 3, 1.75) # strengths (amplitudes)
phs <- c(0, pi/6, pi/4, pi/2) # phase shifts

# create data generating signals
mu <- rep(0, n)
for(j in 1:length(freqs)){
  mu <- mu + amp[j] * sin(2*pi*t*freqs[j] + phs[j])
}
set.seed(1) # set random seed
e <- rnorm(n) # Gaussian error
y <- mu + e # data = mean + error

### FFT of Noise-Free Data ###

# fft of noise-free data
ef <- eegfft(mu, Fs = Fs, upper = 40)
head(ef)
ef[ef$strength > 0.25,]

# plot frequency strength
par(mfrow = c(1,2))
plot(x = ef$frequency, y = ef$strength, t = "b",
      xlab = "Frequency (Hz)",
      ylab = expression("Strength (" * mu * "V)"),
      main = "FFT of Noise-Free Data")

# compare to data generating parameters
cbind(amp, ef$strength[ef$strength > 0.25])
cbind(phs - pi/2, ef$phase[ef$strength > 0.25])

### FFT of Noisy Data ###

# fft of noisy data
ef <- eegfft(y, Fs = Fs, upper = 40)
head(ef)
ef[ef$strength > 0.25,]

# plot frequency strength
plot(x = ef$frequency, y = ef$strength, t = "b",
```

```

xlab = "Frequency (Hz)",
ylab = expression("Strength (" * mu * "V)"),
main = "FFT of Noisy Data")

# compare to data generating parameters
cbind(amp, ef$strength[ef$strength > 0.25])
cbind(phas - pi/2, ef$phase[ef$strength > 0.25])

```

---

eegfilter

*Filters EEG Data*


---

### Description

Low-pass, high-pass, or band-pass filter EEG data using either a Butterworth filter (default) or a finite impulse response (FIR) filter.

### Usage

```

eegfilter(x, Fs, lower, upper, method = "butter",
          order = 3L, forwardreverse = TRUE,
          scale = FALSE, plot = FALSE)

```

### Arguments

x	Vector or matrix (time by channel) of EEG data with n time points.
Fs	Sampling rate of x in Hz.
lower	Lower band in Hz. Smallest frequency to keep.
upper	Upper band in Hz. Largest frequency to keep.
method	Filtering method. Either "butter" for a Butterworth filter or "fir1" for a FIR filter.
order	Order of the filter. See corresponding argument of <a href="#">butter</a> or <a href="#">fir1</a> .
forwardreverse	If TRUE (default), the data are forward and reverse filtered via <a href="#">filtfilt</a> . Otherwise the data are (forward) filtered via <a href="#">filter</a> .
scale	If FALSE (default), the filter is not normalized. Otherwise the magnitude of the center of the first passband is normalized to 1.
plot	If TRUE, the filter is plotted via <a href="#">freqz_plot</a> .

### Details

For a low-pass filter, only enter the upper frequency to keep. For a high-pass filter, only enter the lower frequency to keep. For a band-pass filter, enter both the lower and upper frequency bounds.

### Value

Filtered version of input data.



**Author(s)**

Nathaniel E. Helwig <helwig@umn.edu>

**References**

[http://en.wikipedia.org/wiki/Butterworth\\_filter](http://en.wikipedia.org/wiki/Butterworth_filter)

[http://en.wikipedia.org/wiki/Fir\\_filter](http://en.wikipedia.org/wiki/Fir_filter)

**See Also**

[filter](#), [filtfilt](#), [butter](#), [fir1](#)

**Examples**

```
##### EXAMPLE #####

# create data generating signals
n <- 1000 # 1000 Hz signal
s <- 2 # 2 seconds of data
t <- seq(0, s, length.out = s * n) # time vector
s1 <- sin(2*pi*t) # 1 Hz sinusoid
s5 <- sin(2*pi*t*5) # 5 Hz sinusoid
s10 <- sin(2*pi*t*10) # 10 Hz sinusoid
s20 <- sin(2*pi*t*20) # 20 Hz sinusoid

# create data
set.seed(1) # set random seed
e <- rnorm(s * n, sd = 0.25) # Gaussian error
mu <- s1 + s5 + s10 + s20 # 1 + 5 + 10 + 20 Hz mean
y <- mu + e # data = mean + error

# 4-th order Butterworth filter (2 to 15 Hz band-pass)
yf.but <- eegfilter(y, Fs = n, lower = 2, upper = 15, method = "butter", order = 4)

# 350-th order FIR filter (2 to 15 Hz band-pass)
yf.fir <- eegfilter(y, Fs = n, lower = 2, upper = 15, method = "fir1", order = 350)

# check quality of results
yftrue <- s5 + s10 # true (filtered) mean signal
mean((yf.but - yftrue)^2) # mse between yf.but and yftrue
mean((yf.fir - yftrue)^2) # mse between yf.fir and yftrue

# plot true and estimated filtered signals
plot(t, yftrue, type = "l", lty = 1, lwd = 2, ylim = c(-3, 3))
lines(t, yf.but, col = "blue", lty = 2, lwd = 2)
lines(t, yf.fir, col = "red", lty = 3, lwd = 2)
legend("topright", legend = c("Truth", "Butterworth", "FIR"),
      lty = 1:3, lwd = 2, col = c("black", "blue", "red"), bty = "n")

# power spectral density before and after filtering (dB)
par(mfrow=c(1,3), mar = c(5, 4.5, 4, 2) + 0.1)
```

```

eegpsd(y, Fs = n, upper = 50, t = "b",
      main = "Before Filtering", lwd = 2)
rect(2, -63, 15, 1, col = rgb(0.5,0.5,0.5,1/4))
legend("topright", legend = "2-15 Hz Filter",
      fill = rgb(0.5,0.5,0.5,1/4), bty = "n")
eegpsd(yf.but, Fs = n, upper = 50, t = "b",
      main = "After Butterworth Filter", lwd = 2)
eegpsd(yf.fir, Fs = n, upper = 50, t = "b",
      main = "After FIR Filter", lwd = 2)

# power spectral density before and after filtering (mv^2)
par(mfrow=c(1,3), mar = c(5, 4.5, 4, 2) + 0.1)
eegpsd(y, Fs = n, upper = 50, unit = "mV^2", t = "b",
      main = "Before Filtering", lwd = 2)
rect(2, 0, 15, 1.05, col = rgb(0.5,0.5,0.5,1/4))
legend("topright", legend = "2-15 Hz Filter",
      fill = rgb(0.5,0.5,0.5,1/4), bty = "n")
eegpsd(yf.but, Fs = n, upper = 50, unit = "mV^2", t = "b",
      main = "After Butterworth Filter", lwd = 2)
eegpsd(yf.fir, Fs = n, upper = 50, unit = "mV^2", t = "b",
      main = "After FIR Filter", lwd = 2)

```

---

eeghead

*Dummy Head for 3d EEG Plots*


---

## Description

Contains mesh3d object of dummy head, which is used in the plotting functions [eegcap](#) and [eegspace](#). This is a transformed (translated, rotated, and rescaled) version of the dummyhead object from the Rvcg package.

## Usage

```
data(eeghead)
```

## Format

mesh3d object

## Author(s)

Nathaniel E. Helwig <helwig@umn.edu>

## Source

Created by Nathaniel E. Helwig (2014) using:

Adler, D., Murdoch, D., and others (2014). *rgl: 3D visualization device system (OpenGL)*. <http://CRAN.R-project.org/package=rgl>

Schlager, S. & authors of VCGLIB. (2014). Rvcg: Manipulations of triangular meshes (smoothing, quadric edge collapse decimation, im- and export of various mesh file-formats, cleaning, etc.) based on the VCGLIB API. R package version 0.7.1. <http://CRAN.R-project.org/package=Rvcg>.

## Examples

```
##### EXAMPLE #####
# data(eeghead)
# shade3d(eeghead)
# eeghead$material$color <- rep("black",length(eeghead$material$color))
# wire3d(eeghead)
```

---

eegica

*Independent Component Analysis of EEG Data*

---

## Description

Computes temporal (default) or spatial ICA decomposition of EEG data. Can use Infomax (default), FastICA, or JADE algorithm. ICA computations are conducted via `icaimax`, `icafast`, or `icajade` from the `ica` package.

## Usage

```
eegica(X, nc, center = TRUE, maxit = 100, tol = 1e-6,
       Rmat = diag(nc), type = c("time", "space"),
       method = c("imax", "fast", "jade"), ...)
```

## Arguments

<code>X</code>	Data matrix with <code>n</code> rows (channels) and <code>p</code> columns (time points).
<code>nc</code>	Number of components to extract.
<code>center</code>	If <code>TRUE</code> , columns of <code>X</code> are mean-centered before ICA decomposition.
<code>maxit</code>	Maximum number of algorithm iterations to allow.
<code>tol</code>	Convergence tolerance.
<code>Rmat</code>	Initial estimate of the <code>nc</code> -by- <code>nc</code> orthogonal rotation matrix.
<code>type</code>	Type of ICA decomposition: <code>type="time"</code> extracts temporally independent components, and <code>type="space"</code> extracts spatially independent components.
<code>method</code>	Method for ICA decomposition: <code>method="imax"</code> uses Infomax, <code>method="fast"</code> uses FastICA, and <code>method="jade"</code> uses JADE.
<code>...</code>	Additional inputs to <code>icaimax</code> or <code>icafast</code> function.

## Details

**ICA Model** The ICA model can be written as  $X = \text{tcrossprod}(S, M) + E$ , where columns of  $S$  contain the source signals,  $M$  is the mixing matrix, and columns of  $E$  contain the noise signals. Columns of  $X$  are assumed to have zero mean. The goal is to find the unmixing matrix  $W$  such that columns of  $S = \text{tcrossprod}(X, W)$  are independent as possible.

**Whitening** Without loss of generality, we can write  $M = P \%*\% R$  where  $P$  is a tall matrix and  $R$  is an orthogonal rotation matrix. Letting  $Q$  denote the pseudoinverse of  $P$ , we can whiten the data using  $Y = \text{tcrossprod}(X, Q)$ . The goal is to find the orthogonal rotation matrix  $R$  such that the source signal estimates  $S = Y \%*\% R$  are as independent as possible. Note that  $W = \text{crossprod}(R, Q)$ .

**Infomax** The Infomax approach finds the orthogonal rotation matrix  $R$  that (approximately) maximizes the joint entropy of a nonlinear function of the estimated source signals. See Bell and Sejnowski (1995) and Helwig (in prep) for specifics of algorithms.

**FastICA** The FastICA algorithm finds the orthogonal rotation matrix  $R$  that (approximately) maximizes the negentropy of the estimated source signals. Negentropy is approximated using

$$J(s) = [E\{G(s)\} - E\{G(z)\}]^2$$

where  $E$  denotes the expectation,  $G$  is the contrast function, and  $z$  is a standard normal variable. See Hyvarinen (1999) for specifics of fixed-point algorithm.

**JADE** The JADE approach finds the orthogonal rotation matrix  $R$  that (approximately) diagonalizes the cumulant array of the source signals. See Cardoso and Souloumiac (1993,1996) and Helwig and Hong (2013) for specifics of the JADE algorithm.

## Value

<code>S</code>	Matrix of source signal estimates ( $S=Y\%*\%R$ ).
<code>M</code>	Estimated mixing matrix.
<code>W</code>	Estimated unmixing matrix ( $W=\text{crossprod}(R, Q)$ ).
<code>Y</code>	Whitened data matrix.
<code>Q</code>	Whitening matrix.
<code>R</code>	Orthogonal rotation matrix.
<code>vafs</code>	Variance-accounted-for by each component.
<code>iter</code>	Number of algorithm iterations.
<code>type</code>	ICA type (same as input).
<code>method</code>	ICA method (same as input).

## Note

If `type="time"`, the data matrix is transposed before calling ICA algorithm (i.e.,  $X = t(X)$ ), and the columns of the transposed data matrix are centered.

## Author(s)

Nathaniel E. Helwig <helwig@umn.edu>

## References

- Bell, A.J. & Sejnowski, T.J. (1995). An information-maximization approach to blind separation and blind deconvolution. *Neural Computation*, 7, 1129-1159.
- Cardoso, J.F., & Souloumiac, A. (1993). Blind beamforming for non-Gaussian signals. *IEE Proceedings-F*, 140, 362-370.
- Cardoso, J.F., & Souloumiac, A. (1996). Jacobi angles for simultaneous diagonalization. *SIAM Journal on Matrix Analysis and Applications*, 17, 161-164.
- Helwig, N.E. (2018). *ica: Independent Component Analysis*. <http://CRAN.R-project.org/package=ica>
- Helwig, N.E. & Hong, S. (2013). A critique of Tensor Probabilistic Independent Component Analysis: Implications and recommendations for multi-subject fMRI data analysis. *Journal of Neuroscience Methods*, 213, 263-273.
- Hyvarinen, A. (1999). Fast and robust fixed-point algorithms for independent component analysis. *IEEE Transactions on Neural Networks*, 10, 626-634.

## Examples

```
##### EXAMPLE #####

# get "c" subjects of "eegdata" data
data(eegdata)
idx <- which(eegdata$group=="c")
eegdata <- eegdata[idx,]

# get average data (across subjects)
eegmean <- tapply(eegdata$voltage,list(eegdata$channel,eegdata$time),mean)

# remove ears and nose
acnames <- rownames(eegmean)
idx <- c(which(acnames=="X"),which(acnames=="Y"),which(acnames=="nd"))
eegmean <- eegmean[-idx,]

# get spatial coordinates (for plotting)
data(eegcoord)
cidx <- match(rownames(eegmean),rownames(eegcoord))

# temporal ICA with 4 components
icatime <- eegica(eegmean,4)
icatime$vafs
# quartz()
# par(mfrow=c(4,2))
# tseq <- (0:255)*1000/255
# for(j in 1:4){
#   par(mar=c(5.1,4.6,4.1,2.1))
#   sptitle <- bquote("VAF:  "*(round(icatime$vafs[j],4)))
#   eegtime(tseq,icatime$S[,j],main=bquote("Component  "*(j)),cex.main=1.5)
#   eegspace(eegcoord[cidx,4:5],icatime$M[,j],main=sptitle)
# }

# spatial ICA with 4 components
```

```
icaspace <- eegica(eegmean,4,type="space")
icaspace$vafs
# quartz()
# par(mfrow=c(4,2))
# tseq <- (0:255)*1000/255
# for(j in 1:4){
#   par(mar=c(5.1,4.6,4.1,2.1))
#   sptitle <- bquote("VAF:  "*(round(icaspace$vafs[j],4)))
#   eegtime(tseq,icaspace$M[,j],main=bquote("Component  "*(j)),cex.main=1.5)
#   eegspace(eegcoord[cidx,4:5],icaspace$S[,j],main=sptitle)
# }
```

---

eegmesh

*EEG Cap for Dense Coordinates*

---

## Description

Contains mesh3d object of [eegdense](#), which is used in the plotting function [eegspace](#).

## Usage

```
data(eegmesh)
```

## Format

mesh3d object

## Author(s)

Nathaniel E. Helwig <helwig@umn.edu>

## Source

Created by Nathaniel E. Helwig (2014) using:

Adler, D., Murdoch, D., and others (2014). *rgl: 3D visualization device system (OpenGL)*. <http://CRAN.R-project.org/package=rgl>

Oostenveld, R., and Praamstra, P. (2001). The Five percent electrode system for high-resolution EEG and ERP measurements. *Clinical Neurophysiology*, 112, 713-719.

Schlager, S. & authors of VCGLIB. (2014). Rvcg: Manipulations of triangular meshes (smoothing, quadric edge collapse decimation, im- and export of various mesh file-formats, cleaning, etc.) based on the VCGLIB API. R packge version 0.7.1. <http://CRAN.R-project.org/package=Rvcg>.

**Examples**

```
##### EXAMPLE #####

# data(eegmesh)
# wire3d(eegmesh)
# eegmesh$material$color <- rep("red",length(eegmesh$material$color))
# shade3d(eegmesh)
```

eegpsd

*Plots Power Spectral Density of EEG Data***Description**

Uses a fast discrete Fourier transform ([eegfft](#)) to estimate the power spectral density of EEG data, and plots the power estimate using the [plot](#) (single channel) or [imagebar](#) (multi-channel) function.

**Usage**

```
eegpsd(x, Fs, lower, upper, units = "dB",
       xlab = NULL, ylab = NULL, zlab = NULL, ...)
```

**Arguments**

x	Vector or matrix (time by channel) of EEG data with n time points.
Fs	Sampling rate of x in Hz.
lower	Lower band in Hz. Smallest frequency to keep.
upper	Upper band in Hz. Largest frequency to keep.
units	Units for plot. Options include "dB" for decibals (default), "mV" for microvolts, and "mV^2" for squared microvolts. Note dB = 10*log10(mV^2).
xlab	x-axis label for the plot/image.
ylab	y-axis label for the plot/image.
zlab	z-axis label for the plot/image.
...	Optional inputs for the <a href="#">plot</a> or <a href="#">imagebar</a> function.

**Value**

Produces a plot (single channel) or image (multi-channel).

**Author(s)**

Nathaniel E. Helwig <helwig@umn.edu>

## References

Cooley, James W., and Tukey, John W. (1965) An algorithm for the machine calculation of complex Fourier series, *Math. Comput.* 19(90), 297-301.

Singleton, R. C. (1979) Mixed Radix Fast Fourier Transforms, in *Programs for Digital Signal Processing*, IEEE Digital Signal Processing Committee eds. IEEE Press.

## Examples

```
##### EXAMPLE #####

# create data generating signals
n <- 1000 # 1000 Hz signal
s <- 2 # 2 seconds of data
t <- seq(0, s, length.out = s * n) # time vector
s1 <- sin(2*pi*t) # 1 Hz sinusoid
s5 <- sin(2*pi*t*5) # 5 Hz sinusoid
s10 <- sin(2*pi*t*10) # 10 Hz sinusoid
s20 <- sin(2*pi*t*20) # 20 Hz sinusoid

# create data
set.seed(1) # set random seed
e <- rnorm(s * n, sd = 0.25) # Gaussian error
mu <- s1 + s5 + s10 + s20 # 1 + 5 + 10 + 20 Hz mean
y <- mu + e # data = mean + error

# plot psd (single channel)
eegpsd(y, Fs = n, upper = 30, t = "b")

# plot psd (multi-channel)
ym <- cbind(s1, s5, s10, s20)
eegpsd(ym, Fs = n, upper = 30, units = "mV")
```

---

eegresample

*Change Sampling Rate of EEG Data*

---

## Description

Turn a signal of length N into a signal of length n via linear interpolation.

## Usage

```
eegresample(x, n)
```

## Arguments

x                    Vector or matrix (time by channel) of EEG data with N time points.  
n                    Number of time points for the resampled data.



**Details**

Data are resampled using the "Linear Length Normalization" approach described in Helwig et al. (2011). Let  $\mathbf{x} = (x_1, \dots, x_N)'$  denote the input vector of length  $N$ , and define a vector  $\mathbf{t} = (t_1, \dots, t_n)$  with entries

$$t_i = 1 + (i - 1)\delta$$

for  $i = 1, \dots, n$  where  $\delta = (N - 1)/(n - 1)$ . The resampled vector is calculated as

$$y_i = x_{\lfloor t_i \rfloor} + (x_{\lceil t_i \rceil} - x_{\lfloor t_i \rfloor})(t_i - \lfloor t_i \rfloor)$$

for  $i = 1, \dots, n$  where  $\lfloor \cdot \rfloor$  and  $\lceil \cdot \rceil$  denote the floor and ceiling functions.

**Value**

Resampled version of input data with  $n$  time points.

**Note**

Typical usage is to down-sample (i.e., decrease the sampling rate of) a signal:  $n < N$ .

**Author(s)**

Nathaniel E. Helwig <helwig@umn.edu>

**References**

Helwig, N. E., Hong, S., Hsiao-Wecksler E. T., & Polk, J. D. (2011). Methods to temporally align gait cycle data. *Journal of Biomechanics*, 44(3), 561-566.

**Examples**

```
##### EXAMPLE 1 #####

# create vector with N = 200 time points
N <- 200
x <- sin(4 * pi * seq(0, 1, length.out = N))

# down-sample (i.e., decrease sampling rate) to n = 100
y <- eegresample(x, n = 100)
mean((y - sin(4 * pi * seq(0, 1, length.out = 100)))^2)

# up-sample (i.e., increase sampling rate) to n = 500
z <- eegresample(x, n = 500)
mean((z - sin(4 * pi * seq(0, 1, length.out = 500)))^2)

# plot results
par(mfrow = c(1,3))
plot(x, main = "Original (N = 200)")
plot(y, main = "Down-sampled (n = 100)")
plot(z, main = "Up-sampled (n = 500)")
```

```
##### EXAMPLE 2 #####

# create matrix with N = 500 time points and 2 columns
N <- 500
x <- cbind(sin(2 * pi * seq(0, 1, length.out = N)),
           sin(4 * pi * seq(0, 1, length.out = N)))

# down-sample (i.e., decrease sampling rate) to n = 250
y <- eegresample(x, n = 250)
ytrue <- cbind(sin(2 * pi * seq(0, 1, length.out = 250)),
              sin(4 * pi * seq(0, 1, length.out = 250)))
mean((y - ytrue)^2)

# up-sample (i.e., increase sampling rate) to n = 1000
z <- eegresample(x, n = 1000)
ztrue <- cbind(sin(2 * pi * seq(0, 1, length.out = 1000)),
              sin(4 * pi * seq(0, 1, length.out = 1000)))
mean((z - ztrue)^2)

# plot results
par(mfrow = c(1,3))
plot(x[,1], main = "Original (N = 500)", cex = 0.5)
points(x[,2], pch = 2, col = "blue", cex = 0.5)
plot(y[,1], main = "Down-sampled (n = 250)", cex = 0.5)
points(y[,2], pch = 2, col = "blue", cex = 0.5)
plot(z[,1], main = "Up-sampled (n = 1000)", cex = 0.5)
points(z[,2], pch = 2, col = "blue", cex = 0.5)
```

---

eegsim

---

*Simulate Event-Related Potential EEG Data*


---

## Description

Simulates event-related potential EEG data from hypothetical visual-stimulus ERP study. Data are simulated using a linear combination of five spatiotemporal component functions: P100, N100, P200, N200, and P300 components. User can control the coefficient (weight) given to each component, as well as the time shift (delay) of each component.

## Usage

```
eegsim(channel, time, coefs = rep(1,5), tshift = rep(0,5))
```

## Arguments

channel	Character vector of length n giving EEG channel of simulated data.
time	Numeric vector of length n giving time point of simulated data (should be in interval [0,1]).

coefs	Numeric vector of length 5 giving the coefficients (weights) to use for P100, N100, P200, N200, and P300 components (respectively).
tshift	Numeric vector of length 5 giving the time shifts (delays) to use for P100, N100, P200, N200, and P300 components (respectively).

**Value**

Returns a vector of simulated EEG data corresponding to the input channel(s), time point(s), coefficients, and time shifts.

**Note**

Simulates data for 39 parietal and occipital electrodes: CP1 CP2 CP3 CP4 CP5 CP6 CPZ I1 I2 IZ O1 O2 OZ P1 P2 P3 P4 P5 P6 P7 P8 P9 P10 PO1 PO2 PO3 PO4 PO5 PO6 PO7 PO8 PO9 PO10 POZ PZ TP7 TP8 TP9 TP10

Returns simulated value of 0 for other electrodes.

**Author(s)**

Nathaniel E. Helwig <helwig@umn.edu>

**References**

Created by Nathaniel E. Helwig (2014) using data from:

Bache, K. & Lichman, M. (2013). UCI Machine Learning Repository [<http://archive.ics.uci.edu/ml>]. Irvine, CA: University of California, School of Information and Computer Science.

Begleiter, H. *Neurodynamics Laboratory*. State University of New York Health Center at Brooklyn. <http://www.downstate.edu/hbnl/>

Ingber, L. (1997). Statistical mechanics of neocortical interactions: Canonical momenta indicators of electroencephalography. *Physical Review E*, 55, 4578-4593.

Ingber, L. (1998). Statistical mechanics of neocortical interactions: Training and testing canonical momenta indicators of EEG. *Mathematical Computer Modelling*, 27, 33-64.

**Examples**

```
##### EXAMPLE #####

### plot spatiotemporal component functions

# data(eegcoord)
# chnames <- rownames(eegcoord)
# tseq <- seq(0,1,length.out=200)

# quartz(width=18,height=6)
# layout(matrix(c(1,2,3,4,5,6,7,8,9,10,11,11), 2, 6, byrow = TRUE))

# eegspace(eegcoord[,4:5],pls(chnames),cex.point=1,main=expression(psi[p1]),cex.main=2,vlim=c(-3,9))
# eegtime(tseq,plt(tseq),ylim=c(-1,1),asp=1/2,main=expression(tau[p1]),cex.main=2,
#         xlab="Time After Stimulus (sec)")
```

```

# eegspace(eegcoord[,4:5],p2s(chnames),cex.point=1,main=expression(psi[p2]),cex.main=2,vlim=c(-3,9))
# eegtime(tseq,p2t(tseq),ylim=c(-1,1),asp=1/2,main=expression(tau[p2]),cex.main=2,
#       xlab="Time After Stimulus (sec)")
# eegspace(eegcoord[,4:5],p3s(chnames),cex.point=1,main=expression(psi[p3]),cex.main=2,vlim=c(-3,9))
# eegtime(tseq,p3t(tseq),ylim=c(-1,1),asp=1/2,main=expression(tau[p3]),cex.main=2,
#       xlab="Time After Stimulus (sec)")
# eegspace(eegcoord[,4:5],n1s(chnames),cex.point=1,main=expression(psi[n1]),cex.main=2,vlim=c(-3,9))
# eegtime(tseq,n1t(tseq),ylim=c(-1,1),asp=1/2,main=expression(tau[n1]),cex.main=2,
#       xlab="Time After Stimulus (sec)")
# eegspace(eegcoord[,4:5],n2s(chnames),cex.point=1,main=expression(psi[n2]),cex.main=2,vlim=c(-3,9))
# eegtime(tseq,n2t(tseq),ylim=c(-1,1),asp=1/2,main=expression(tau[n2]),cex.main=2,
#       xlab="Time After Stimulus (sec)")
# plot(seq(-10,10),seq(-10,10),type="n",axes=FALSE,xlab="",ylab="")
# text(0,8,labels=expression(omega[p1]*" = "*psi[p1]*tau[p1]),cex=2)
# text(0,4,labels=expression(omega[n1]*" = "*psi[n1]*tau[n1]),cex=2)
# text(0,0,labels=expression(omega[p2]*" = "*psi[p2]*tau[p2]),cex=2)
# text(0,-4,labels=expression(omega[n2]*" = "*psi[n2]*tau[n2]),cex=2)
# text(0,-8,labels=expression(omega[p3]*" = "*psi[p3]*tau[p3]),cex=2)

### plot simulated data at various time points

# quartz(width=15,height=3)
# tseq <- c(50,150,250,350,450)/1000
# par(mfrow=c(1,5))
# for(j in 1:5){
#   eegspace(eegcoord[,4:5],eegsim(chnames,rep(tseq[j],87)),vlim=c(-6.8,5.5),
#         main=paste(tseq[j]*1000," ms"),cex.main=2)
# }

```

---

eegsmooth

*Spatial and/or Temporal Smoothing of EEG Data*


---

## Description

Smooths single- or multi-channel electroencephalography (EEG) with respect to space and/or time. Uses the [big spline](#), [big tps](#), and [big ssa](#) functions (from [big splines](#) package) for smoothing.

## Usage

```
eegsmooth(voltage, space = NULL, time = NULL, nknots = NULL,
          rparm = NULL, lambdas = NULL, skip.iter = TRUE,
          se.fit = FALSE, rseed = 1234)
```

## Arguments

**voltage**                      Vector of recorded EEG voltage at each row in space.

space	Matrix of electrode coordinates (in three-dimensions) at which EEG was recorded. If space=NULL, data are temporally smoothed only.
time	Vector of time points at which EEG was recorded. If time=NULL, data are spatially smoothed only.
nknots	Number of knots to sample for smoothing. Positive integer.
rparm	Rounding parameter(s) to use for smoothing. See Notes and Examples.
lambdas	Smoothing parameter(s) to use for smoothing.
skip.iter	If FALSE, iterative spatial-temporal smoothing is skipped. Ignored if space=NULL or time=NULL.
se.fit	If TRUE, standard errors of smoothed values are calculated.
rseed	Random seed to use for knot selection. Set rseed=NULL to obtain different knots each time, or set rseed to any positive integer to use a different random seed.

**Value**

For temporal smoothing only: an object of class "bigspline" (see [bigspline](#)).

For spatial smoothing only: an object of class "bigtps" (see [bigtps](#)).

For spatial-temporal smoothing: an object of class "bigssa" (see [bigssa](#)).

**Note**

For temporal smoothing only (i.e., space=NULL), the input rparm should be a positive scalar less than 1. Larger values produce faster (but less accurate) approximations. Default is 0.01, which I recommend for temporal smoothing; rparm=0.005 may be needed for particularly rough signals, and rparm=0.02 could work for smoother signals.

For spatial smoothing only (i.e., time=NULL), the input rparm should be a positive scalar giving the rounding unit for the spatial coordinates. For example, rparm=0.1 rounds each coordinate to the nearest 0.1 (same as round(space, 1)).

For spatial-temporal smoothing (i.e., both space and time are non-null), the input rparm should be a list of the form rparm=list(space=0.1, time=0.01), where the 0.1 and 0.01 can be replaced by your desired rounding parameters.

Setting rparm=NA will use the full data solution; this is more computationally expensive, and typically produces a solution very similar to using rparm=0.01 (see references).

**Author(s)**

Nathaniel E. Helwig <helwig@umn.edu>

**References**

Helwig, N. E. (2013). *Fast and stable smoothing spline analysis of variance models for large samples with applications to electroencephalography data analysis*. Unpublished doctoral dissertation. University of Illinois at Urbana-Champaign.

Helwig, N.E. (2015). *bigsplines: Smoothing Splines for Large Samples*. <http://CRAN.R-project.org/package=bigsplines>

Helwig, N. E. & Ma, P. (2015). Fast and stable multiple smoothing parameter selection in smoothing spline analysis of variance models with large samples. *Journal of Computational and Graphical Statistics*, 24(3), 715-732.

Helwig, N. E. & Ma, P. (2016). Smoothing spline ANOVA for super large samples: Scalable computation via rounding parameters. *Statistics and Its Interface*, 9(4), 433-444.

## Examples

```
##### EXAMPLE 1: Temporal #####

# get "PZ" electrode of "c" subjects in "eegdata" data
data(eegdata)
idx <- which(eegdata$channel=="PZ" & eegdata$group=="c")
eegdata <- eegdata[idx,]

# temporal smoothing
eegmod <- eegsmooth(eegdata$voltage,time=eegdata$time)

# define data for prediction
time <- seq(min(eegdata$time),max(eegdata$time),length.out=100)
yhat <- predict(eegmod,newdata=time,se.fit=TRUE)

# plot results using eegtime
eegtime(time*1000/255,yhat$fit,voltageSE=yhat$se.fit,ylim=c(-4,4),main="Pz")

##### EXAMPLE 2: Spatial #####

# get time point 65 (approx 250 ms) of "c" subjects in "eegdata" data
data(eegdata)
idx <- which(eegdata$time==65L & eegdata$group=="c")
eegdata <- eegdata[idx,]

# remove ears, nose, and reference (Cz)
idx <- c(which(eegdata$channel=="X"),which(eegdata$channel=="Y"),
        which(eegdata$channel=="nd"),which(eegdata$channel=="Cz"))
eegdata <- eegdata[-idx,]

# match to eeg coordinates
data(eegcoord)
cidx <- match(eegdata$channel,rownames(eegcoord))

# spatial smoothing
eegmod <- eegsmooth(eegdata$voltage,space=eegcoord[cidx,1:3])

# use dense cap for prediction
mycap <- levels(factor(eegdata$channel))
ix <- eegcapdense(mycap,type="2d",index=TRUE)
data(eegdense)
space <- eegdense[ix,1:3]
yhat <- predict(eegmod,newdata=space)
```

```

# plot results using eegspace
#eegspace(space,yhat)
eegspace(eegdense[ix,4:5],yhat)

##### EXAMPLE 3: Spatial-Temporal (not run) #####

# # get "c" subjects of "eegdata" data
# data(eegdata)
# idx <- which(eegdata$group=="c")
# eegdata <- eegdata[idx,]

# # remove ears, nose, and reference (Cz)
# idx <- c(which(eegdata$channel=="X"),which(eegdata$channel=="Y"),
#         which(eegdata$channel=="nd"),which(eegdata$channel=="Cz"))
# eegdata <- eegdata[-idx,]

# # match to eeg coordinates
# data(eegcoord)
# cidx <- match(eegdata$channel,rownames(eegcoord))

# # spatial-temporal smoothing
# eegmod <- eegsmooth(eegdata$voltage,space=eegcoord[cidx,1:3],time=eegdata$time)

# # time main effect
# newdata <- list(time=seq(min(eegdata$time),max(eegdata$time),length.out=100))
# yhat <- predict(eegmod,newdata=newdata,se.fit=TRUE,include="time")
# eegtime(newdata$time,yhat$fit,voltageSE=yhat$se.fit,ylim=c(-2,4),main="Time Main Effect")

# # space main effect
# mycap <- levels(factor(eegdata$channel))
# ix <- eegcapdense(mycap,type="2d",index=TRUE)
# data(eegdense)
# newdata <- list(space=eegdense[ix,1:3])
# yhat <- predict(eegmod,newdata=newdata,include="space")
# eegspace(newdata$space,yhat)

# # interaction effect (spatial map at time point 65)
# newdata <- list(space=eegdense[ix,1:3],time=rep(65,nrow(eegdense[ix,])))
# yhat <- predict(eegmod,newdata=newdata,include="space:time")
# eegspace(newdata$space,yhat)

# # full prediction (spatial map at time point 65)
# newdata <- list(space=eegdense[ix,1:3],time=rep(65,nrow(eegdense[ix,])))
# yhat <- predict(eegmod,newdata=newdata)
# eegspace(newdata$space,yhat)

```

**Description**

Creates plot of multi-channel electroencephalography (EEG) spatial map. User can control the plot type (2d or 3d), the colormap, color, etc.

**Usage**

```
eegspace(space, voltage, vlim = NULL, mycolors = NULL, ncolor = 25,
         colorbar = TRUE, nctick = 5, rtick = 1, cex.axis = 1,
         barloc = NULL, colorlab = NULL, colorlabline = 3, cex.lab = 1,
         plotaxes = FALSE, main = "", xyzlab = NULL, cex.point = 1,
         cex.main = 1, nose = TRUE, ears = TRUE, head = TRUE,
         col.head = "AntiqueWhite", mar = NULL, ...)
```

**Arguments**

space	Matrix of input electrode coordinates (3d or 2d).
voltage	Vector of recorded EEG voltage at each row in space.
vlim	Two-element vector giving the limits to use when mapping voltage to colors in mycolors. Default is vlim=range(voltage).
mycolors	Character vector of colors to use for color mapping (such that length(mycolors)<=ncolor). Default: mycolors=c("blueviolet", "blue", "cyan", "green", "yellow", "orange", "red").
ncolor	Number of colors to use in mapping (positive integer).
colorbar	If TRUE, colorbar is plotted.
nctick	Approximate number of ticks for colorbar. Ignored if colorbar=FALSE.
rtick	Round tick labels to given decimal. Ignored if colorbar=FALSE.
cex.axis	Cex of axis ticks for colorbar. Ignored if colorbar=FALSE.
barloc	Character vector giving location of color bar. See Notes.
colorlab	Character vector giving label for color bar. Ignored if colorbar=FALSE.
colorlabline	Line number for color bar label (for input to <code>mtext</code> ).
cex.lab	Cex of axis labels for colorbar. Ignored if colorbar=FALSE.
plotaxes	If TRUE, axes labels are plotted. Ignored for 3d plots.
main	Plot title. Default is no title.
xyzlab	Axis labels to use for plot. If type="2d", then xyzlab should be two-element character vector giving x and y axis labels. If type="3d", then xyzlab should be three-element character vector giving x, y, and z axis labels.
cex.point	Cex for plotted electrodes.
cex.main	Cex for plot title. Ignored if main=NULL.
nose	If TRUE, triangle is plotted to represent the subject's nose. Ignored if ncol(space)==3.
ears	If TRUE, ovals are plotted to represent the subject's ears. Ignored if ncol(space)==3.
head	If TRUE, head is plotted. Ignored if type="2d".
col.head	Color for dummy head in 3d plot. Ignored if type="2d".
mar	Margins to use for plot (see par).
...	Optional inputs for plot or lines function.



**Value**

Produces plot of EEG spatial map with NULL return value.

**Note**

For 3d plots, `barloc` can be one of four options: "backright", "backleft", "frontright", or "frontleft". For 2d plots, `barloc` can be either "right" or "left".

Currently supports spatial maps registered to the 84-channel cap produced by `eegcap` and `eegcoord`.

**Author(s)**

Nathaniel E. Helwig <helwig@umn.edu>

**References**

Bache, K. & Lichman, M. (2013). UCI Machine Learning Repository [<http://archive.ics.uci.edu/ml>]. Irvine, CA: University of California, School of Information and Computer Science.

Begleiter, H. *Neurodynamics Laboratory*. State University of New York Health Center at Brooklyn. <http://www.downstate.edu/hbnl/>

Ingber, L. (1997). Statistical mechanics of neocortical interactions: Canonical momenta indicators of electroencephalography. *Physical Review E*, 55, 4578-4593.

Ingber, L. (1998). Statistical mechanics of neocortical interactions: Training and testing canonical momenta indicators of EEG. *Mathematical Computer Modelling*, 27, 33-64.

**Examples**

```
##### EXAMPLE #####

# get time point 65 (approx 250 ms) from "eegdata" data
data(eegdata)
idx <- which(eegdata$time==65L)
eegdata <- eegdata[idx,]

# get average spatial map
eegmean <- tapply(eegdata$voltag, list(eegdata$channel, eegdata$group), mean)

# remove ears and nose
acnames <- rownames(eegmean)
idx <- c(which(acnames=="X"), which(acnames=="Y"), which(acnames=="nd"), which(acnames=="Cz"))
eegmean <- eegmean[-idx,]

# match to eeg coordinates
data(eegcoord)
cidx <- match(rownames(eegmean), rownames(eegcoord))

# # plot average control voltage in 3d
# open3d()
# eegspace(eegcoord[cidx, 1:3], eegmean[, 2])
```

```
# plot average control voltage in 2d
eegspace(eegcoord[cidx,4:5],eegmean[,2])

# # change 3d bar location and use play3d to rotate (not run)
# open3d()
# par3d(windowRect=c(0,0,600,600))
# eegspace(eegcoord[cidx,1:3],eegmean[,2],barloc="frontleft")
# play3d(spin3d(axis=c(0,0,1),rpm=5),duration=20)

# change 2d bar location
eegspace(eegcoord[cidx,4:5],eegmean[,2],barloc="left")
```

---

eegtime

*Plots Single-Channel EEG Time Course*


---

## Description

Creates plot of single-channel electroencephalography (EEG) time course with optional confidence interval. User can control the plot orientation, line types, line colors, etc.

## Usage

```
eegtime(time, voltage, flipvoltage = TRUE, vlty = 1, vlwd = 2,
        vcol = "blue", voltageSE = NULL, slty = NA, slwd = 1,
        scol = "cyan", salpha = 0.65, conflevel = 0.95,
        plotzero = TRUE, zlty = 1, zlwd = 0.5, zcol = "black",
        xlim = NULL, ylim = NULL, xlab = NULL, ylab = NULL,
        nxtick = 6, nytick = 6, xticks = NULL, yticks = NULL,
        add = FALSE, ...)
```

## Arguments

time	Vector of time points at which EEG was recorded.
voltage	Vector of recorded EEG voltage at each point in time.
flipvoltage	If TRUE, negative voltages are plotted upwards.
vlty	Line type for voltage.
vlwd	Line width for voltage.
vcol	Line color for voltage.
voltageSE	Vector of standard errors of EEG voltage at each point in time.
slty	Line type for voltageSE. If slty=NA (default) shaded polygons are plotted.
slwd	Line width for voltageSE. Ignored if slty=NA.
scol	Polygon or line color for voltageSE.
salpha	Transparency value for voltageSE polygon (only used if slty=NA).
conflevel	Confidence level to use for confidence intervals. Default forms 95% CI.

plotzero	If TRUE, horizontal reference line is plotted at 0 volts.
zlty	Line type for reference line. Ignored if plotzero=FALSE.
zlwd	Line width for reference line. Ignored if plotzero=FALSE.
zcol	Line color for reference line. Ignored if plotzero=FALSE.
xlim	Plot limits for time.
ylim	Plot limits for voltage.
xlab	Plot label for time.
ylab	Plot label for voltage.
nxtick	Approximate number of axis ticks for time.
nytick	Approximate number of axis ticks voltage.
xticks	x-axis ticks for time (overrides nxtick).
yticks	y-axis ticks voltage (overrides nytick).
add	If TRUE, lines are added to current plot; otherwise a new plot is created.
...	Optional inputs for plot or lines function.

**Value**

Produces plot of EEG time course with NULL return value.

**Note**

Confidence intervals are formed using the normal (Gaussian) distribution.

**Author(s)**

Nathaniel E. Helwig <helwig@umn.edu>

**References**

- Bache, K. & Lichman, M. (2013). UCI Machine Learning Repository [<http://archive.ics.uci.edu/ml>]. Irvine, CA: University of California, School of Information and Computer Science.
- Begleiter, H. *Neurodynamics Laboratory*. State University of New York Health Center at Brooklyn. <http://www.downstate.edu/hbnl/>
- Ingber, L. (1997). Statistical mechanics of neocortical interactions: Canonical momenta indicators of electroencephalography. *Physical Review E*, 55, 4578-4593.
- Ingber, L. (1998). Statistical mechanics of neocortical interactions: Training and testing canonical momenta indicators of EEG. *Mathematical Computer Modelling*, 27, 33-64.

**Examples**

```
##### EXAMPLE #####

# get "PZ" electrode from "eegdata" data
data(eegdata)
idx <- which(eegdata$channel=="PZ")
eegdata <- eegdata[idx,]

# get average and standard error (note se=sd/sqrt(n))
eegmean <- tapply(eegdata$voltage,list(eegdata$time,eegdata$group),mean)
eegse <- tapply(eegdata$voltage,list(eegdata$time,eegdata$group),sd)/sqrt(50)

# plot results with legend
tseq <- seq(0,1000,length.out=256)
eegtime(tseq,eegmean[,2],voltageSE=eegse[,2],ylim=c(-10,6),main="Pz")
eegtime(tseq,eegmean[,1],vltty=2,vcol="red",voltageSE=eegse[,1],scol="pink",add=TRUE)
legend("bottomright",c("controls","alcoholics"),lty=c(1,2),
      lwd=c(2,2),col=c("blue","red"),bty="n")
```

---

eegtimemc

*Plots Multi-Channel EEG Time Course*


---

**Description**

Creates plot of multi-channel electroencephalography (EEG) time courses with subplots positioned according to electrode locations. User can control the plot orientation, line types, line colors, etc.

**Usage**

```
eegtimemc(time, voltmat, channel, size = c(0.75,0.75),
          vadj = 0.5, hadj = 0.5, xlab = "", ylab = "",
          voltSE = NULL, vltty = 1, slty = NA, vlwd = 1,
          slwd = 1, vcol = "blue", scol = "cyan", ...)
```

**Arguments**

time	Vector of time points at which EEG was recorded.
voltmat	Matrix of multi-channel EEG voltages (time by channel).
channel	Character vector giving name of channel for each column of voltmat.
size	Relative size of each subplot.
vadj	Vertical adjustment for each subplot.
hadj	Horizontal adjustment for each subplot.
xlab	X-axis label for each subplot.
ylab	Y-axis label for each subplot.
voltSE	Matrix of voltage standard errors (same size as voltmat).

vlt	Line type for voltmat.
sly	Line type for voltSE. If sly=NA (default) shaded polygons are plotted.
vlw	Line width for voltmat.
slw	Line width for voltSE. Ignored if sly=NA.
vcol	Line color for voltmat.
scol	Polygon or line color for voltSE.
...	Optional inputs for eegtime function.

**Value**

Produces plot of EEG time course with NULL return value.

**Note**

Currently supports 84 scalp electrodes (plus ears and nose): A1 A2 AF1 AF2 AF3 AF4 AF5 AF6 AF7 AF8 AFZ C1 C2 C3 C4 C5 C6 CP1 CP2 CP3 CP4 CP5 CP6 CPZ CZ F1 F2 F3 F4 F5 F6 F7 F8 F9 F10 FC1 FC2 FC3 FC4 FC5 FC6 FCZ FP1 FP2 FPZ FT7 FT8 FT9 FT10 FZ I1 I2 IZ NZ O1 O2 OZ P1 P2 P3 P4 P5 P6 P7 P8 P9 P10 PO1 PO2 PO3 PO4 PO5 PO6 PO7 PO8 PO9 PO10 POZ PZ T7 T8 T9 T10 TP7 TP8 TP9 TP10

Subplots are created using eegtime, so input ... can be any optional input for eegtime.

Inspired by Frank Harrell's subplot function (in Hmisc package).

**Author(s)**

Nathaniel E. Helwig <helwig@umn.edu>

**References**

Bache, K. & Lichman, M. (2013). UCI Machine Learning Repository [<http://archive.ics.uci.edu/ml>]. Irvine, CA: University of California, School of Information and Computer Science.

Begleiter, H. *Neurodynamics Laboratory*. State University of New York Health Center at Brooklyn. <http://www.downstate.edu/hbnl/>

Harrell, F., Dupont, C., and Others. *Hmisc: Harrell Miscellaneous*. <http://CRAN.R-project.org/package=Hmisc>

Ingber, L. (1997). Statistical mechanics of neocortical interactions: Canonical momenta indicators of electroencephalography. *Physical Review E*, 55, 4578-4593.

Ingber, L. (1998). Statistical mechanics of neocortical interactions: Training and testing canonical momenta indicators of EEG. *Mathematical Computer Modelling*, 27, 33-64.

**Examples**

```
##### EXAMPLE #####
# # get control ("c") data from "eegdata" data
# data(eegdata)
# idx <- which(eegdata$group=="c")
# eegdata <- eegdata[idx,]
```

```
# # get average
# eegmean <- tapply(eegdata$voltage,list(eegdata$time,eegdata$channel),mean)
# eegse <- tapply(eegdata$voltage,list(eegdata$time,eegdata$channel),sd)/sqrt(50)

# # plot time course for all electrodes
# dev.new(height=15,width=15, noRStudioGD = TRUE)
# tseq <- seq(0,1000,length.out=256)
# eegtimemc(tseq,eegmean,colnames(eegmean),ylim=c(-11,14),voltSE=eegse)
```

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